

Epilepsy, Respiration, and Cortical Excitability

Martina Saltafossi^{1,2}, Teresa Berther^{1,2}, Gian Marco Duma³, Simone Cuozzo³, Luc Wilson⁴, Paolo Bonanni³, Joachim Gross^{1,2}, Daniel S. Kluger^{1,2}

¹Institute for Biomagnetism and Biosignal Analysis, University of Münster, Münster, Germany
²Otto Creutzfeldt Center for Cognitive and Behavioral Neuroscience, University of Münster, Münster, Germany
³Scientific Institute IRCCS E. Medea, Epilepsy and Clinical Neurophysiology Unit, Conegliano, Italy
⁴McConnell Brain Imaging Centre, Montréal Neurological Institute, McGill University, Montréal, Canada

Background

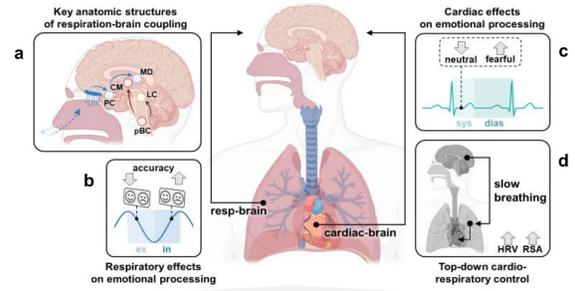


Fig. 1. Respiratory coupling to brain function and behaviour¹. a, Nasal respiration activates olfactory bulb mechanoreceptors, shaping neural oscillations, while brainstem generators regulate arousal via the thalamus and locus coeruleus^{2,3}. b & c, Respiratory and cardiac phases influence sensory^{4,5} and emotional processing^{6,7}. d, Respiration serves as a crucial physiological modulator, as it can control the (para)sympathetic tone through respiratory sinus arrhythmia⁸.

- Respiration drives neural signaling by modulating both oscillatory and non-oscillatory (1/f slope) dynamics⁹
- Epilepsy often involves dysregulation of excitation-inhibition (E:I) balance, reflected in alteration of the 1/f slope^{10,11}
- A case report on focal epilepsy demonstrated respiration phase-locked shifts of E:I balance and their role in the timing of interictal epileptiform discharges¹²
- The extent to which respiration affects cortical excitability and oscillatory activity in a larger epilepsy cohort remains unclear

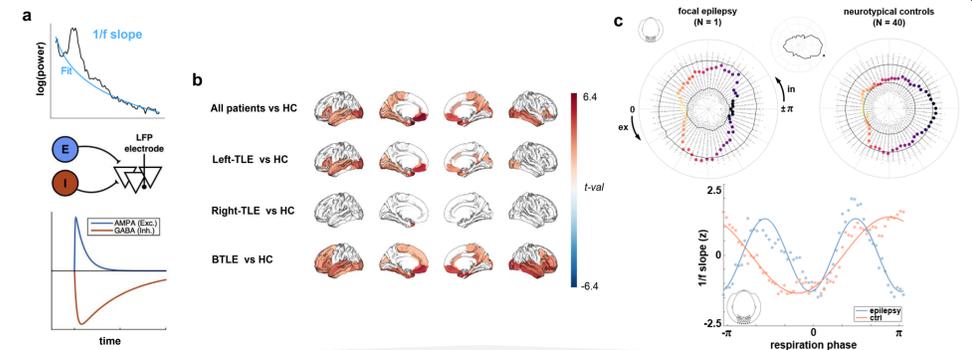


Fig. 2. E:I balance, epilepsy and their link to respiration. a, The 1/f spectral slope of the electrophysiological power spectrum, representing the non-oscillatory, scale-free component of neural activity, relates to cognitive and perceptual states. It reflects synaptic current integration, with excitatory currents producing a flatter PSD and inhibitory currents resulting in a steeper PSD, depending on their relative dominance^{13,14}. b, Patients with temporal lobe epilepsy exhibit a larger aperiodic exponent (i.e., $E < 1$), primarily localised in the temporal, dorsal-frontal, and cingulate regions of the brain¹¹. c, Changes in the 1/f slope are phase-locked to respiration in both epilepsy and neurotypical population. However, in epilepsy, this relationship appears to function differently, potentially reflecting altered neural dynamics associated with the disorder¹².

Methods

Epilepsy patients

- The majority of the clinical sample consists of patients with focal and bilateral TLE, followed by those with FLE and OLE
- Detailed clinical information, including epilepsy type, age of onset, current age, medication, sex, and other relevant factors, will be available soon and will inform the analyses

Data acquisition

- Long-term video-EEG monitoring with cardio-respiratory polygraphy
- Low-density EEG: N channels = 15 - 29
- Respiration via abdominal belt
- 1 hour of resting state -like data extracted (before sleep)

Preprocessing and analyses

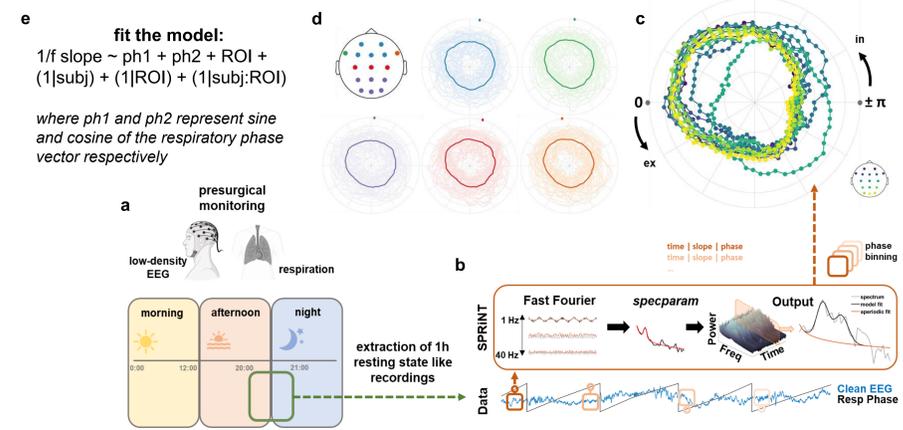


Fig. 3. Methods synopsis 1/f slope ~ respiration. a, 1 hour of interictal EEG and peripheral signals were extracted from long-term monitoring. b, After cleaning the data, single channel time series were subjected to the SPRINT algorithm¹⁵. Using a moving window, estimates of the aperiodic component of the Fourier-transformed neural data are obtained every 250ms. For each moving-window centre, the corresponding respiratory phase was extracted. This yielded quasi-continuous, respiration phase-resolved courses of 1/f slope per channel^{9,12}. c & d, Averaged phase ($n = 60$)-binned slopes are computed for each channel and for each ROIs (e.g. lobes) per patient. e, Linear mixed effect models (LMEM) will be employed to test the influence of respiratory phase on 1/f slope.

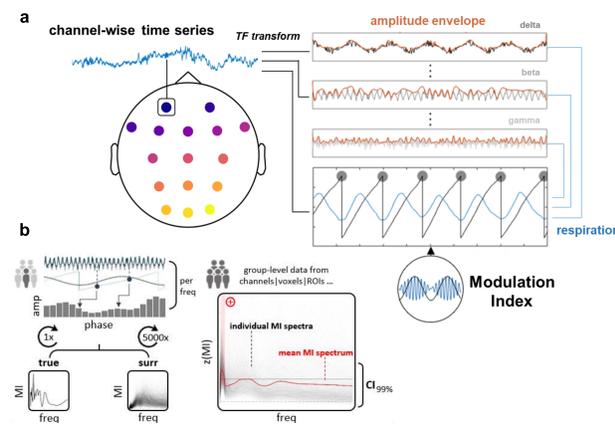


Fig. 4. Modulation Index analysis. a, MI quantifies the extent to which the amplitude envelopes of frequency-specific brain oscillations are modulated by respiration. We computed modulation indices for each channel, frequency, and patient¹⁶. b, Statistical testing for MI will involve creating $k = 5000$ surrogate respiration time series using the iterated amplitude-adjusted Fourier transform (IAAFT)¹⁷. These surrogates serve as a null distribution against which the observed MI values are compared.

Preliminary results

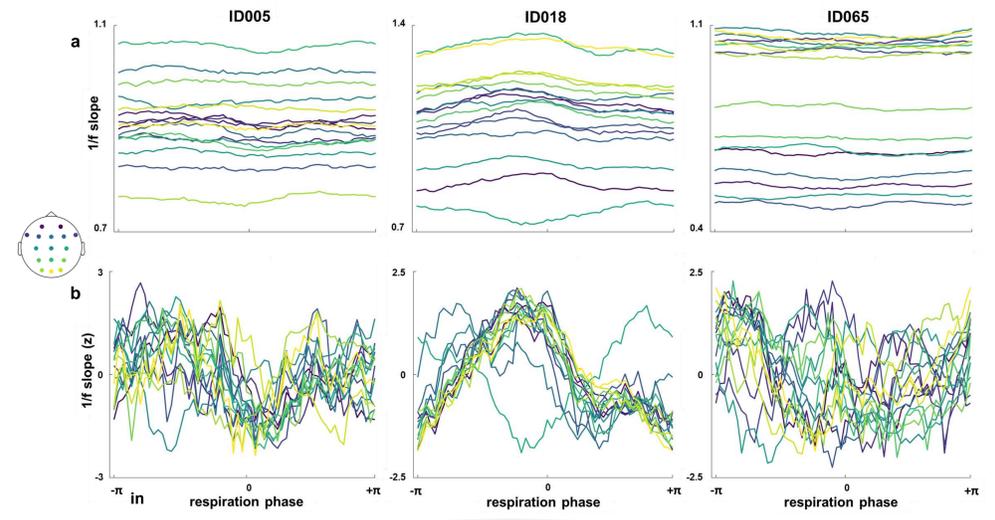


Fig. 5. 1/f slope ~ respiration per channel. a, Plots showing baseline variability across 16 channels for three exemplary patients. b, Corresponding plots illustrating modulation within the respiratory cycle, where the 1/f slope is normalised across phase bins. Each patient's channel layout was subsampled to a common set of 16 channels.

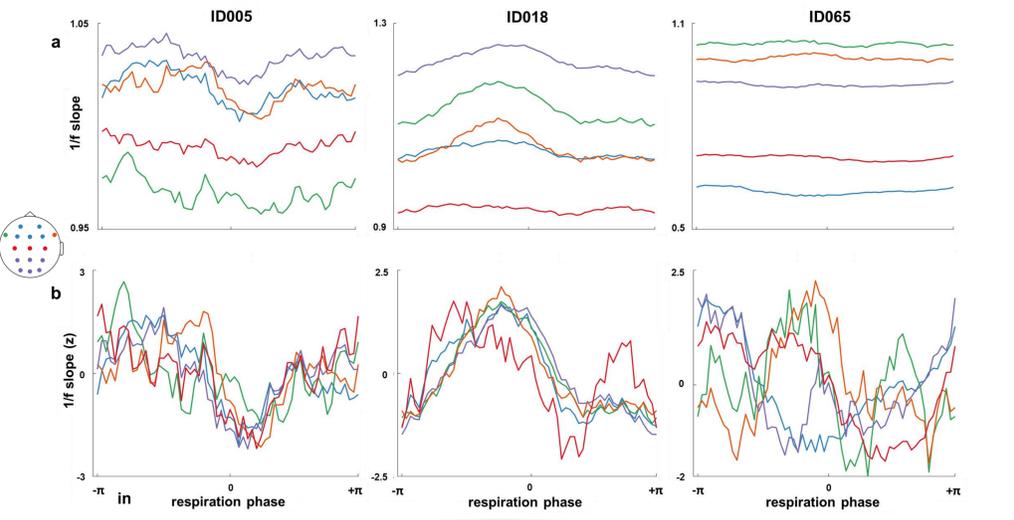


Fig. 6. 1/f slope ~ respiration per ROI. a, Plots showing baseline variability of the 1/f slope across five ROIs (frontal, left-temporal, right-temporal, central, and parieto-occipital) for three exemplary patients. b, Corresponding plots illustrating modulation within the respiratory cycle, with the 1/f slope normalised across phase bins. Note that here the number of channels per ROI may vary depending on the individual montage ($n = 15-29$).

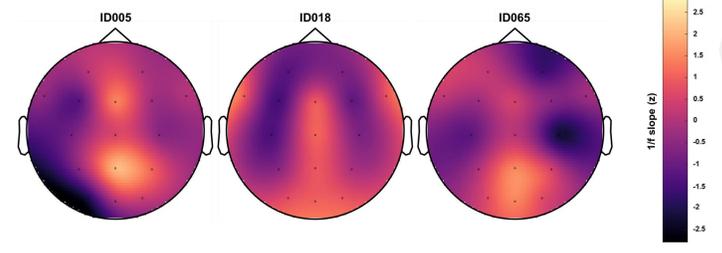


Fig. 7. Topographic organisation of E:I balance. The three topographies depict the spatial distribution of the 1/f slope, averaged across respiratory phases. Darker colours indicate greater excitability, while brighter colours reflect a shift toward inhibition.

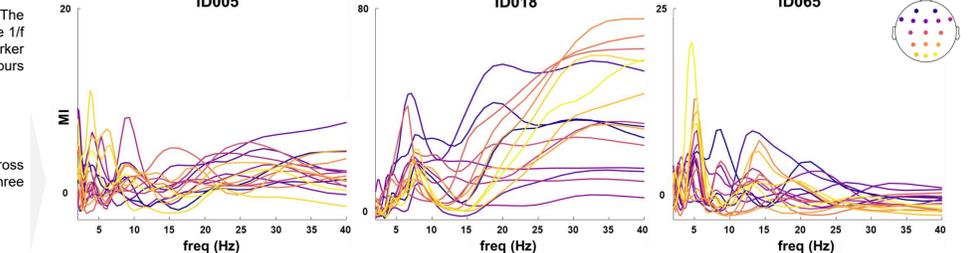


Fig. 8. Modulation Index. Plots display MI values across frequencies (2-40 Hz) for each channel ($n = 16$) in three exemplary patients.

Discussion

- Power spectral phenomena (oscillatory and non-oscillatory activity) are more useful biomarkers in the interictal phase since they are ubiquitous and consistently available for quantification, in contrast to the sporadically occurring interictal epileptic discharges and seizures¹⁸
- These cortical dynamics are coupled to respiration in (at least) two different ways
 - phase-amplitude coupling driven by infraslow oscillations within OB¹⁹
 - CO₂-induced changes in tissue pH linked to excitability changes (via adenosine/ATP levels)²⁰⁻²³
- Respiratory alkalosis (i.e., elevated arterial pH) triggers hyperventilation-provoked seizures in rats and humans²⁴. Additionally, altered respiratory-related brain pulsations (i.e., mechanical stimulation) may contribute to epileptic pathophysiology by disrupting CSF homeostasis and neural oscillations²⁵
- Future directions:
 - tailor analyses to clinical data (e.g. seizure onset foci)
 - investigate brain-respiration coupling during sleep

References

1. Saltafossi et al., J Aff Dis, 2025 | 2. Brændholt et al., NBBR, 2023 | 3. Kluger et al., J Neurosci, 2024 | 4. Saltafossi et al., bioRxiv, 2025 | 5. Saltafossi et al., Biol Psychol, 2023 | 6. Garfinkel et al., J Neurosci, 2014 | 7. Zelano et al., J Neurosci, 2016 | 8. Zaccaro et al., Front Hum Neurosci, 2018 | 9. Kluger et al., Nat Comm, 2023 | 10. Van Heumen et al., Front Hum Neurosci, 2021 | 11. Duma et al., Brain Comm, 2024 | 12. Kluger et al., Med Comm, acc | 13. Gao et al., Neurolmage, 2017 | 14. Donoghue et al., Nat Neur, 2020 | 15. Wilson et al., eLife, 2022 | 16. Kluger et al., PLoS Biol, 2021 | 17. Theiler et al., Physica D: Nonlin Phen, 1992 | 18. Latreille et al., Epilepsia, 2024 | 19. Ito et al., Nat Comm, 2014 | 20. Chesler, Physiol Rev, 2003 | 21. Lee et al., Brain Res, 1996 | 22. Ito et al., J Cereb Blood Flow Metab, 2003 | 23. Dulla et al., Neuron, 2005 | 24. Salvati et al., eLife, 2022 | 25. Elabasy et al., Sci Rep, 2023

Transdiagnostic Brain-Body | Epilepsy (case study) | Further reading

Respiration & multisensory integration | Cardiac phases & multisensory integration

Saltafossi et al., bioRxiv 2025 | Saltafossi et al., Biol Psychol 2023

Contact: martinassaltafossi.bsky.social | martina.saltafossi@uni-muenster.de

Saltafossi et al., J Aff Dis 2025 | Kluger et al., Med Comm accepted